

# Enhancing the *in vivo* detection of cancer by manipulating magnetic fields applied to tumor targeting superparamagnetic iron oxide nanoparticles

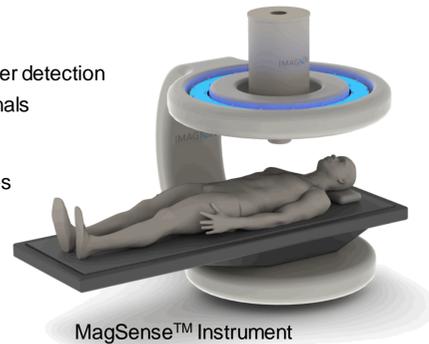
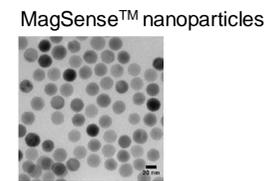
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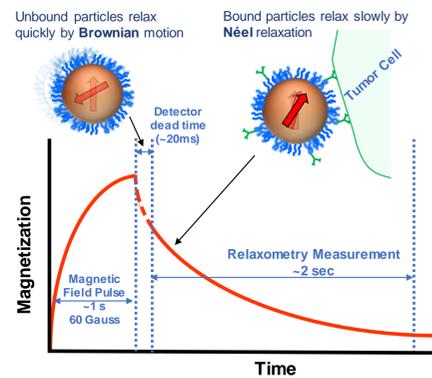


## Introduction

- The MagSense™ platform consists of superconducting quantum interference devices (SQUIDs) to detect tumor targeted iron oxide nanoparticles (NPs) that are specifically bound to cancer cells. The detection relies on SQUIDs high sensitivity to magnetic field produced by the superparamagnetic relaxation (SPMR) of the NPs.
- Proof of concept demonstrates specific detection of HER-2 positive breast cancer cells *in vitro* and *in vivo*.
- Current efforts are focused to:
  - Improve the lower limit of SPMR Cancer detection
  - Reduce the influence of off-target signals



## SPMR Background



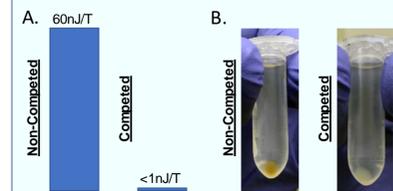
### *In vivo* SPMR Cancer Detection

- Inject mAb conjugated NPs
- Apply small magnetizing pulse
- NPs relax to their equilibrium states
  - Brownian motion of unbound NPs [fast and undetectable]
  - Néel relaxation of NPs bound to cells [slow and detectable]

**SPMR ONLY DETECTS NPs BOUND TO CANCER CELLS/TISSUES**

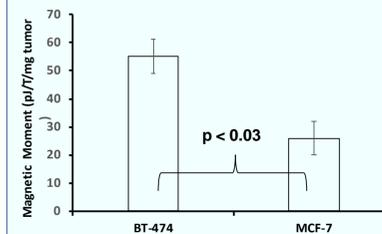
## Proof-of-Concept SPMR specific cancer detection

### *In Vitro* Cell Competition



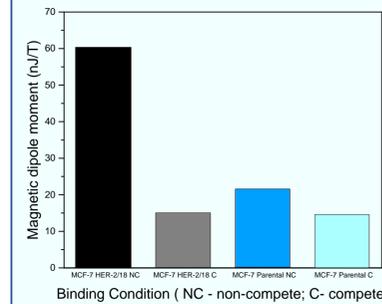
Competitive binding of anti-HER2 conjugated NPs to MCF7/HER2-18 cells as measured by **A.** the MagSense™ instrument and confirmed by **B.** digital photography.

### *In Vivo* Cell Specificity



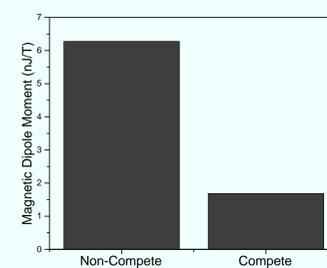
The strength of the magnetic dipole generated by the MagSense-Anti-HER2 particles is dependent on the level of HER2 expression on the cell surface.

### *In Vitro* Cell Specificity



Competitive binding of anti-HER2 conjugated NPs can be correlated to the expression of HER2 on cells. MagSense™ measurements of MCF7/HER2-18 and parental MCF7 cells.

### *In Vivo* Cell Competition

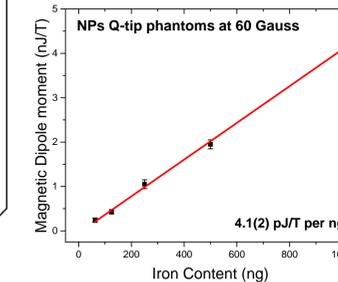
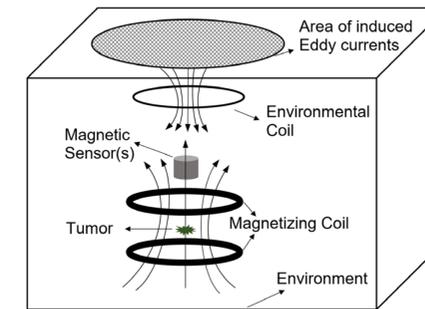


*In vivo* competition study showed ~4X magnetic dipole signal in non-compete mouse vs. compete mouse.

## Reducing the influence of the environmental background

**The Problem:** The magnetization pulse induces non-specific magnetic fields (Eddy currents in the conductive environment), that increase instrument dead time, limit dynamic range, and lower the sensitivity.

**Solution:** Generate a field of opposite polarity to cancel Eddy currents

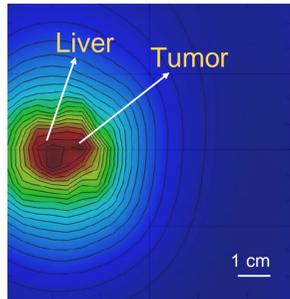
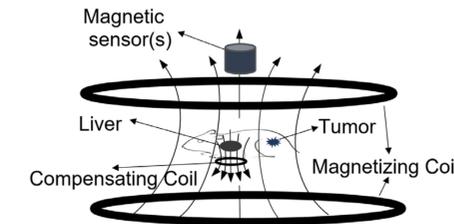


- 4-fold Improvement on the lower limit of *in vitro* detection from 250 ng to 62.5 ng of Fe
- Reached, *in vitro* sensitivity to 5,000 BT474 targeted cells ( $5 \times 10^4$  nps/cell (achieved) at  $3 \times 10^9$  nps/ $\mu\text{g}$  of  $\text{Fe}_3\text{O}_4$ )
- Projected, *in vivo* sensitivity at 100,000 cancer cells (e.g., in lymph nodes at 100% delivery at 3-cm depth)
- Projected, detection *in vivo* tumor size of 2.5  $\text{mm}^3$  (at 4% tumor delivery at 3-cm depth, e.g., breast cancer)

## Improving tumor detectability

**The Problem:** SPMR signals at off-target sites (liver and spleen) influence tumor detection

**Solution:** Compensate the magnetic field at off-target sites



- 6-fold reduction of the Liver signal from  $3.3 \times 10^2$  to  $0.56 \times 10^2$  nJ/T
- Resolving a Tumor of 10% of a liver at 2cm away from the liver
- Projected, 10-fold reduction of liver signal with a better coil design

## Summary and Conclusion

- We presented the proof-of-concept SPMR specific cancer detection *in vivo* and *in vitro*
- Demonstrated improvement in tumor detectability *in vitro* by reducing signals at off-target sites
- An improvement of the lower limit of detection to 5,000 BT474 cells *in vitro* was presented
- We project sensitivity to 100,000 cells (100% delivery) and 2.5  $\text{mm}^3$  tumor size (at 4% delivery) at 3-cm depth - primary breast tumors and sentinel lymph nodes detection
- Future work: Improvements on MagSense™ Instrument and NPs to allow for detection at larger depth